

# Denoising in Digital Radiographic Images Using a Deep Convolutional Neural Network

**Karin Toepfer, PhD, Lori Barski, MS,  
Levon Vogelsang, PhD, William Sehnert, PhD**

Carestream Health  
Rochester, New York  
December, 2020

# Outline

---

- Background
- Purpose
- Materials and methods
- Results
- Conclusion

# Background

---

- Best practice medical X-ray imaging employs the principle of ALARA “as low as reasonably achievable” for dose selection
- This leads to inherently noisy images with dose just high enough to confidently achieve a diagnosis\*
- Medical image processing often includes noise suppression with traditional methods leading to some loss in fine image detail
- Noise reduction with deep convolutional neural networks (CNN) has been shown to preserve more image detail\*\*
- This can lead to improved image quality, improved contrast-to-noise, easier to read radiographs and the potential for additional dose reduction

\* <https://www.carestream.com/blog/2020/04/21/understanding-and-managing-noise-sources-in-x-ray-imaging/>

\*\* Hu Chen, Yi Zhang, "Low-Dose CT with a Residual Encoder-Decoder Convolutional Neural Network (RED-CNN)", 2017, <https://arxiv.org/ftp/arxiv/papers/1702/1702.00288.pdf>

# Purpose

To characterize image quality improvements and dose reduction of denoising based on a deep convolutional neural network (CNN) in radiographic imaging

Current image processing

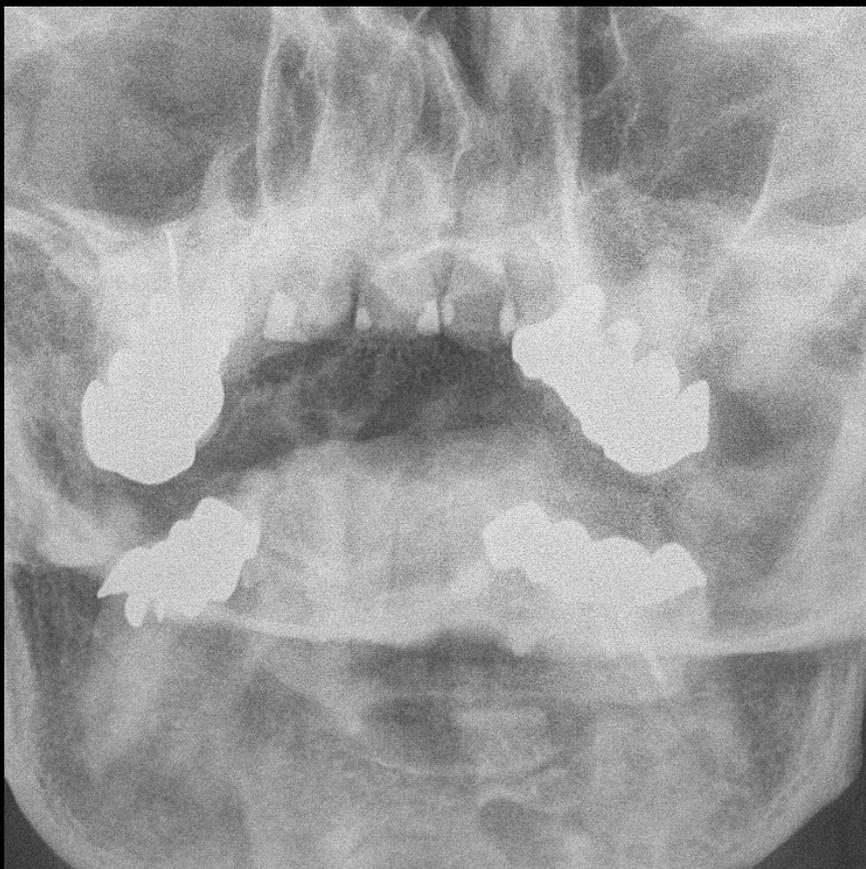
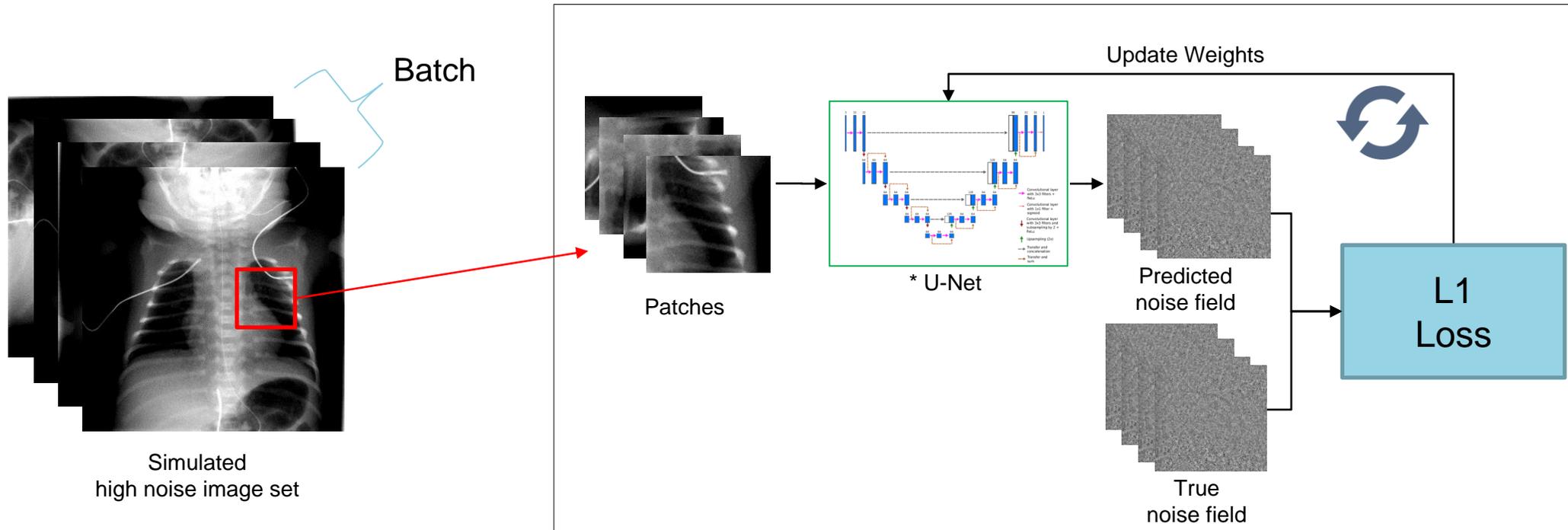


Image processing with denoising by CNN

---

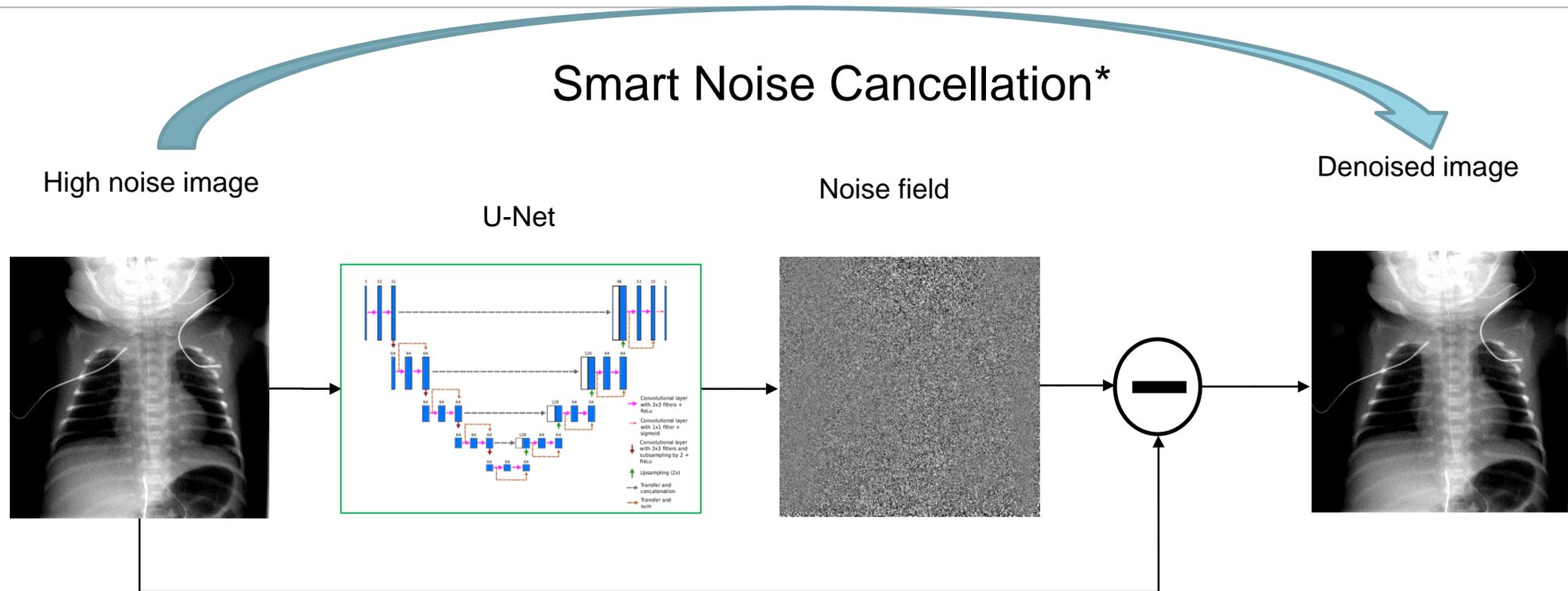
# MATERIALS AND METHODS

# Model Description for Deep CNN



- Training set: 250+ image / noise field pairs per detector type
- Batch size: 32 images
- 480 randomly sampled 128×128 patches per image
- Trained for 200 epochs for a total of > 24 million evaluated unique patches
- Models were developed independently for Carestream DRX family of detectors, based on choice of scintillator, pixel pitch and electronic noise (referred to as detector type)

# Prediction



\* Creating the denoised image from the noisy image using the U-Net is referred to as Smart Noise Cancellation throughout the presentation

# Terminology

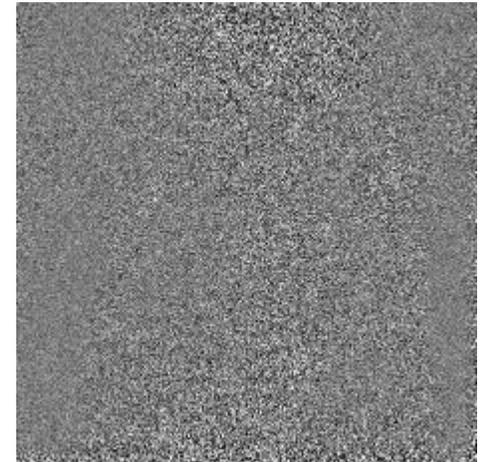
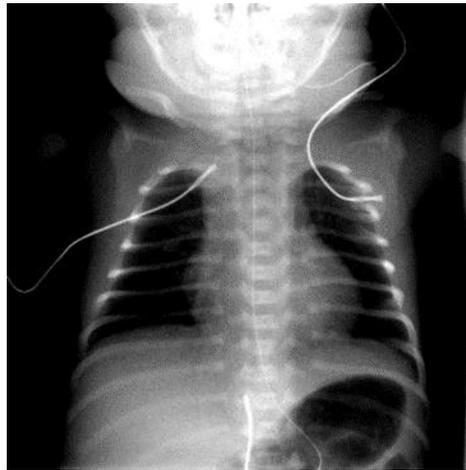
---

- Smart Noise Cancellation: Denoising module based on deep convolutional neural network
- Eclipse: The engine behind Carestream's Radiography Software. Eclipse uses AI technology and proprietary algorithms to significantly increase the value of the entire imaging chain from capture to diagnosis. Eclipse powers features for imaging intelligence, workflow efficiency and healthcare analytics
- Eclipse + Smart Noise Cancellation: The Eclipse engine powers our new feature called Smart Noise Cancellation

# Training Data

- 250+ anonymized raw clinical images typical for general radiography and pediatrics
- Training pairs were generated using noise simulations\*

Input images	Aim images	Aim noise field
Image simulations with the appropriate amount of added noise corresponding to lower dose	Original images scaled by the dose reduction factor without added noise	Difference between input and aim images



\* US Patent 7480,365 B1, K. Topfer, J. Ellinwood, "Dose Reduced Digital Medical Image Simulations"

# Testing Data

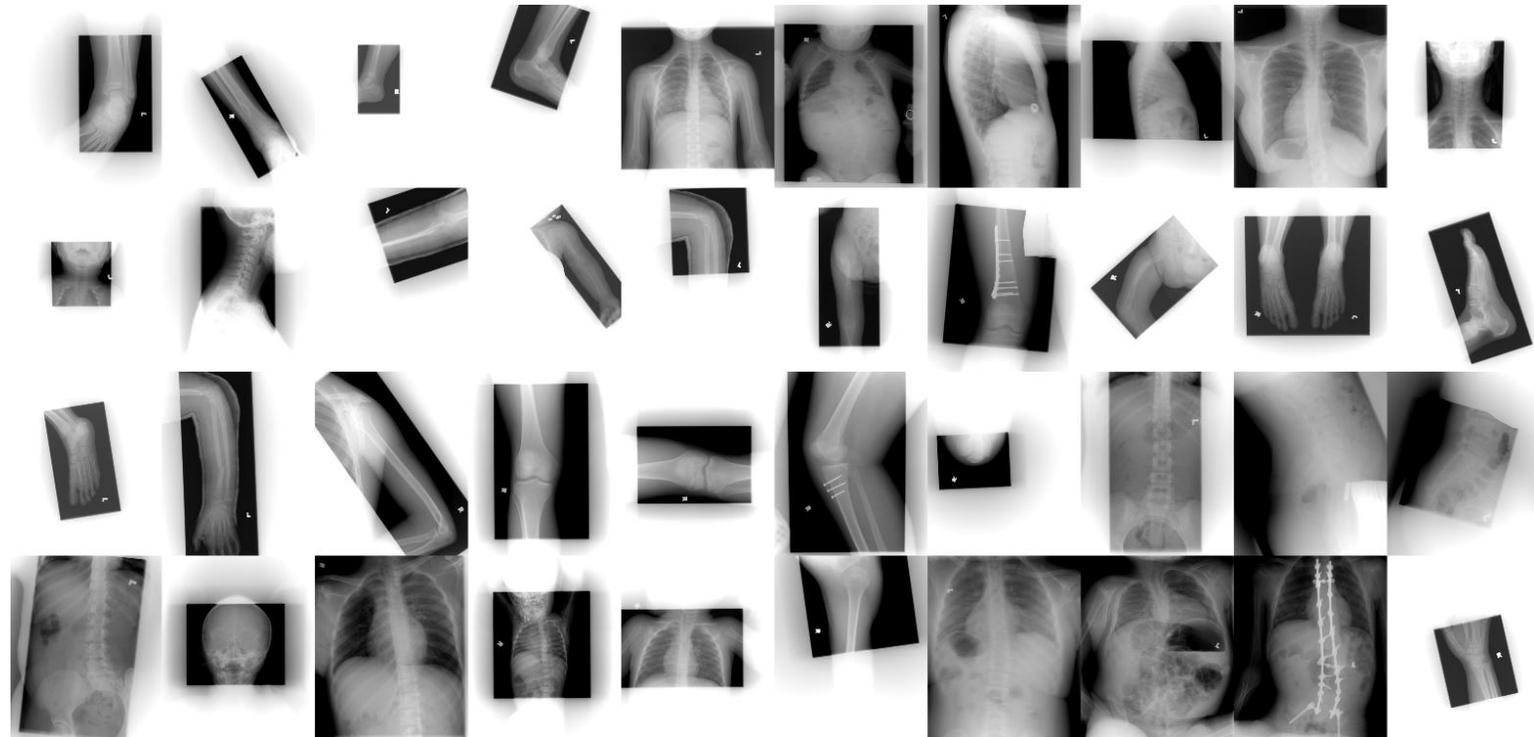
---

- Over 400 test images per detector type
  - Anonymized raw clinical images typical for general radiography and pediatrics independent of training set
  - Test phantom set for quantitative evaluation
  - Simulated disease features on clinical backgrounds
- Test images and associated quantitative analyses can help to define the potential dose reduction

# Testing Data – Clinical Images

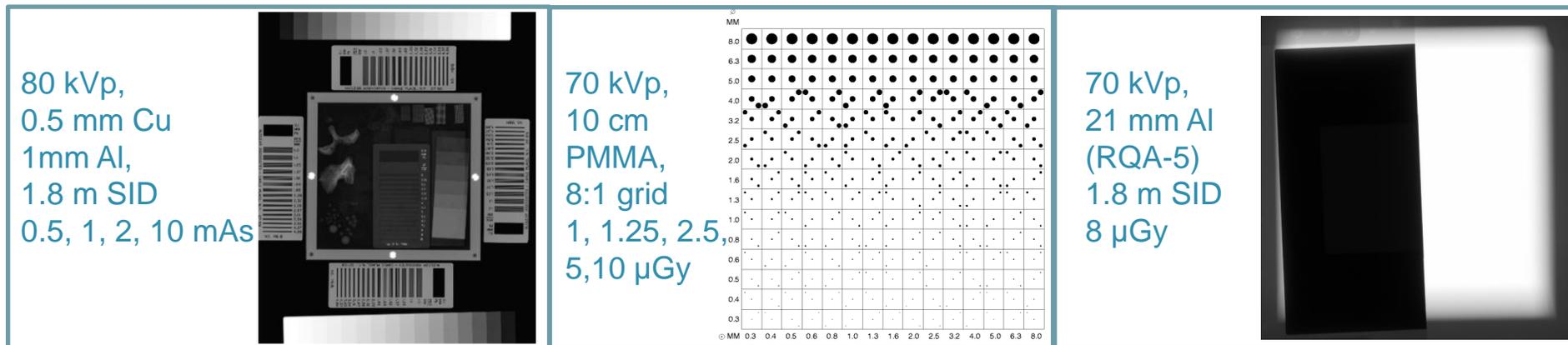
- Smart Noise Cancellation was assessed visually in clinical images
- Visual evaluation of the predicted noise field for lack of residual edges and structure
- Comparison of processed images with and without the Smart Noise Cancellation module for sharpness, noise, low-contrast and fine detail, and image artifacts

Montage of typical clinical test images



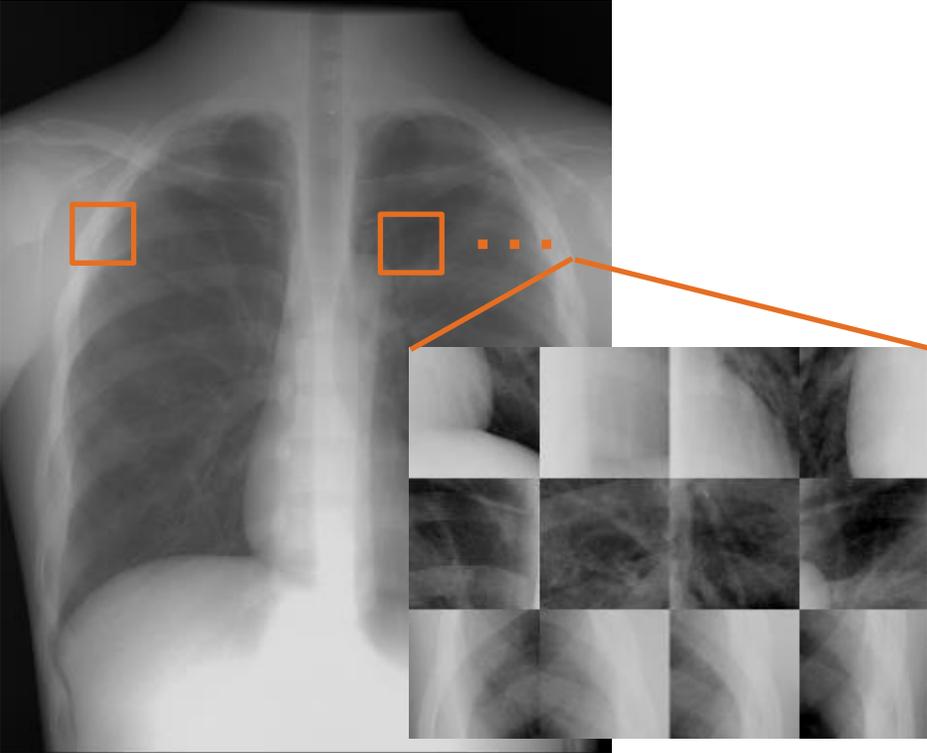
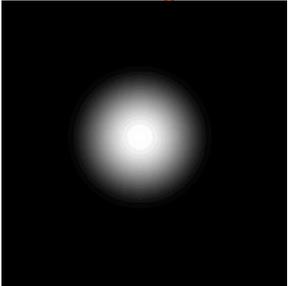
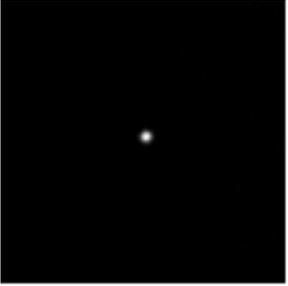
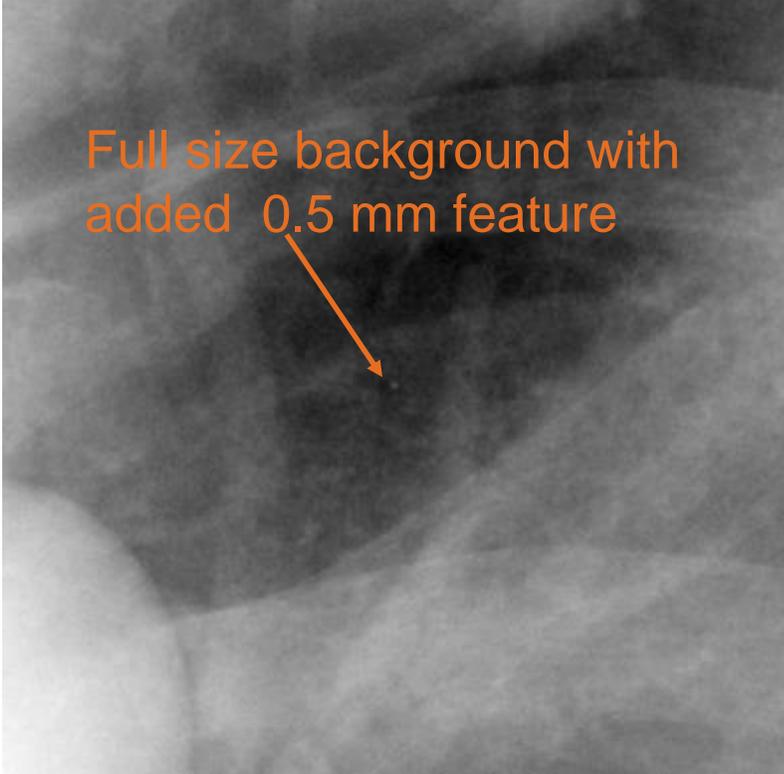
# Testing Data – Phantom Set and Techniques

Step tablets	Artinis CDRAD phantom*	MTF target according to IEC 62220-1
Uniform area noise reduction	Contrast-detail evaluation	High contrast sharpness



\* R. van der Burght, M. Floor, M. Thijssen and R. Bijkerk. Manual CDRAD 2.0 Phantom & Analyser software version 2.1, Rev. 1709, Artinis Medical Systems, 2017

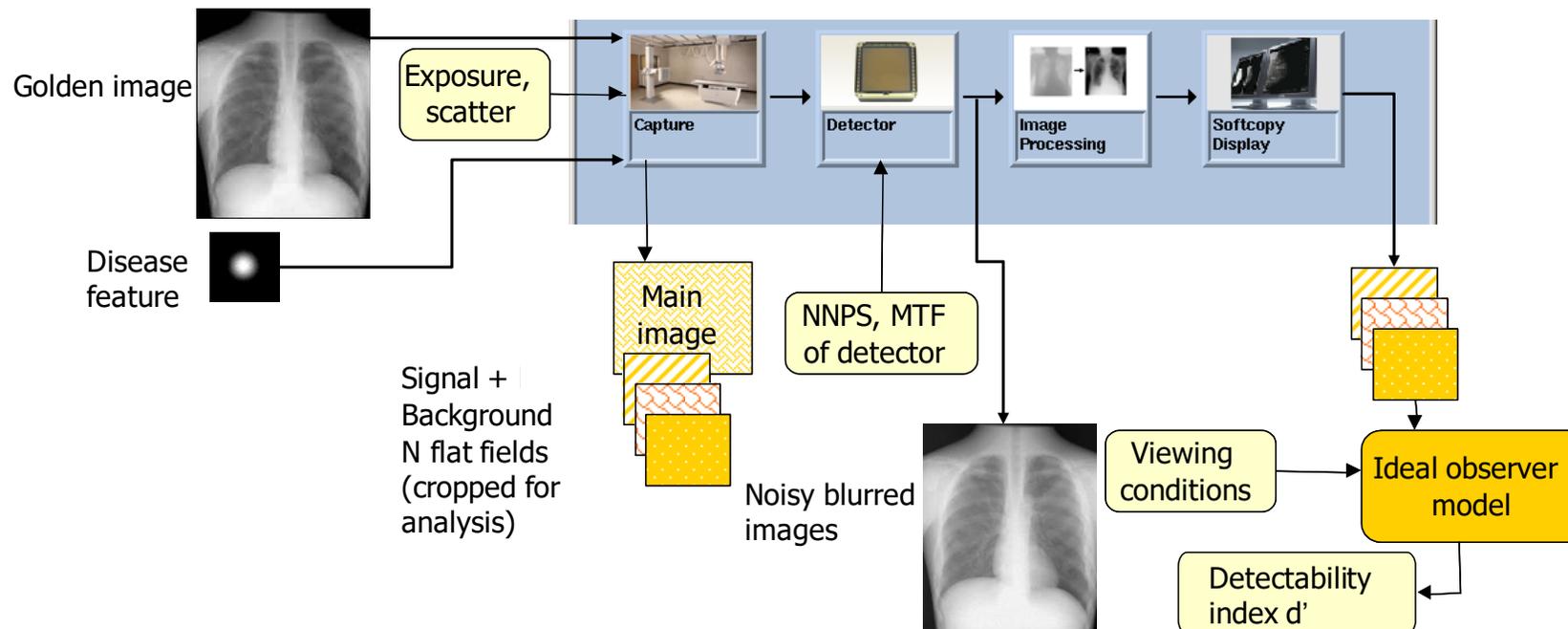
# Testing Data – Disease Feature Simulation

“Golden” clinical image	Disease Features	Simulated image captures
Chest image without noise, scatter and blur; 12 backgrounds were extracted for analysis	10 mm lung nodule* and 0.5 mm high-contrast feature at 2 contrast levels	Combined backgrounds and disease features
	<p data-bbox="1131 622 1505 661">10 mm lung nodule*</p>  <p data-bbox="1029 968 1569 1006">0.5 mm high contrast feature</p> 	 <p data-bbox="1735 729 2333 839">Full size background with added 0.5 mm feature</p>

\*E. Samei, M. J. Flynn, and W. R. Eyler, “Simulation of subtle lung nodules in projection chest radiography,” *Radiology*, 202, 117-124 (1997)

# Disease Feature Simulation System Model

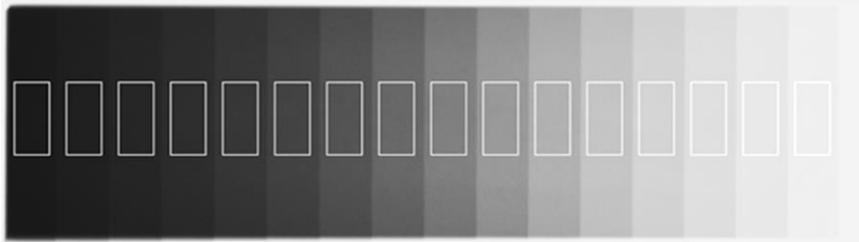
- Simulation of the entire image chain from “golden” images with added disease features\*
- Adding scatter, detector noise and blur, corresponding to 800 and 400 speed captures on a specific detector type
- Image chain includes image processing, with and without Smart Noise Cancellation, display and viewing conditions
- Channelized Hotelling observer => detection of disease features, detectability index  $d'$



\*Töpfer, K., Keelan, B. W., Sugiro, F., “An advanced system model for the prediction of the clinical task performance of radiographic systems,” Proc. SPIE 6515, 651512-1-12 (2007)

# Evaluation Metrics

- Image Noise



- Analysis on linear raw images
- Robust standard deviation and mean of the marked ROIs was obtained
- Plot of noise vs mean, analysis in linear exposure space

- Contrast-Detail Analysis

- Automatic scoring of CDRAD images using CDRAD Analyser 2.0 software
- 10 replicates per exposure, 5 e-5 significance level
- Feature size,  $D_i$ , vs. lowest visible contrast,  $C_i$
- Quality score  $IQF_{inv}$ :

$$IQF_{inv} = \frac{100}{\sum_{i=1}^{15} C_i \times D_{i,th}}$$

$D_{i,th}$ : threshold diameter of hole (mm), detail  
 $C_i$ : depth of hole (mm), contrast

- Sharpness – Modulation Transfer Function (MTF)

- Analysis on linear raw images
- MTF analysis according to IEC 62220-1 Standard
- MTF vs spatial frequency under RQA-5 beam conditions

- Detectability Index  $d'$

- Average over results from 12 chest backgrounds
- Calculated for 10 mm lung nodule and 0.5 mm feature at 1x and 1.3x contrast
- Calculated at 400 and 800 speed with Eclipse processing and compared with 800 speed with Eclipse + Smart Noise Cancellation



---

# RESULTS

# Results – Visual Evaluation of Noise Field

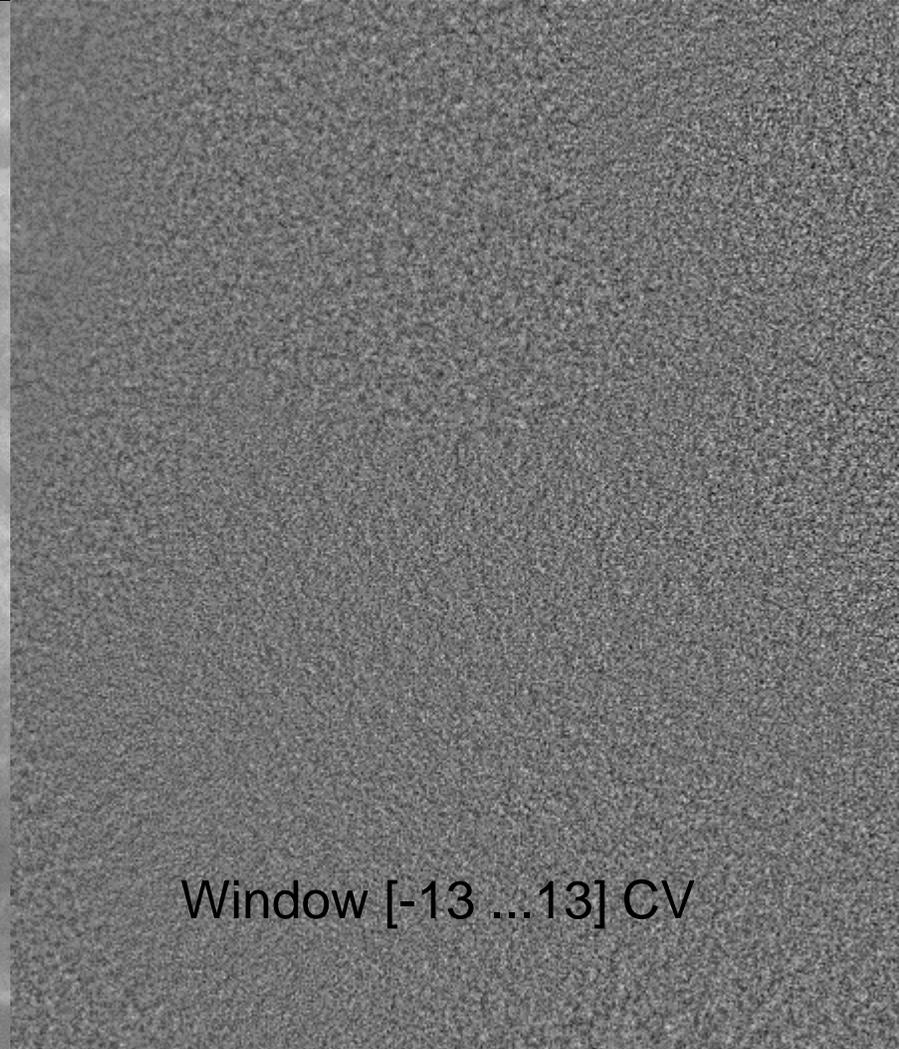
Noisy image



Image after Smart Noise Cancellation

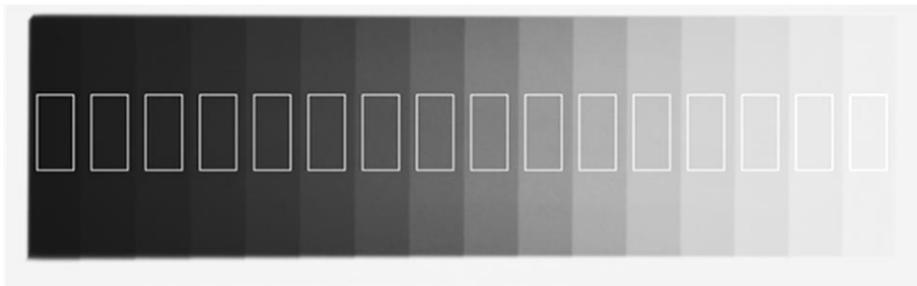


Predicted noise field

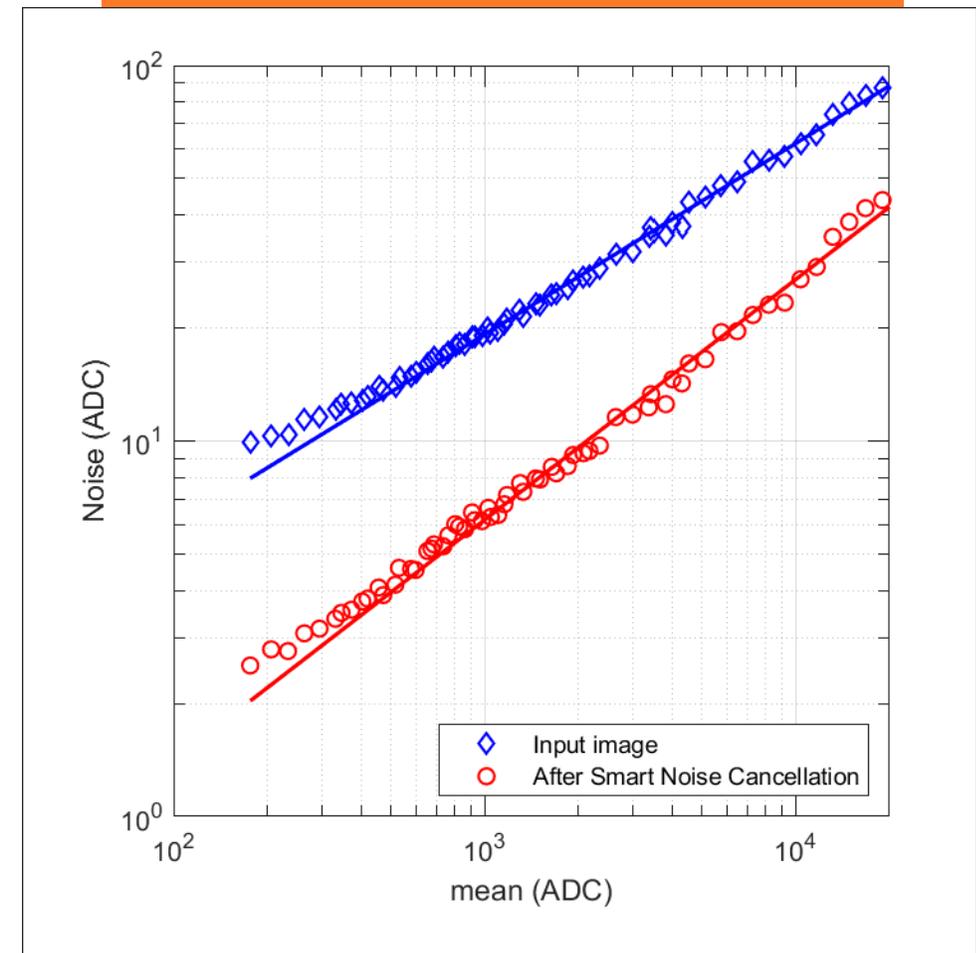


# Results – Uniform Area Noise Reduction

- Analysis of AI step tablet at 4 different exposure levels
- Comparison before and after Smart Noise Cancellation, results displayed for DRX Plus 3543C
- The solid blue line before noise reduction indicates quantum limited behavior ( $\text{Noise} \propto \text{mean}^{0.5}$ )
- Flat field noise reduction ranged between 4x at low exposures and 2x at higher exposures!
- In terms of quantum noise, 2x noise reduction corresponds to the image appearance of a 4x higher exposure!

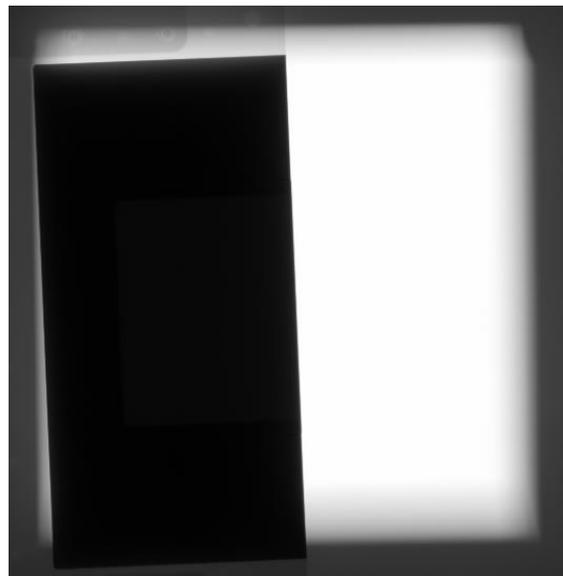


2x to 4x noise reduction with Smart Noise Cancellation



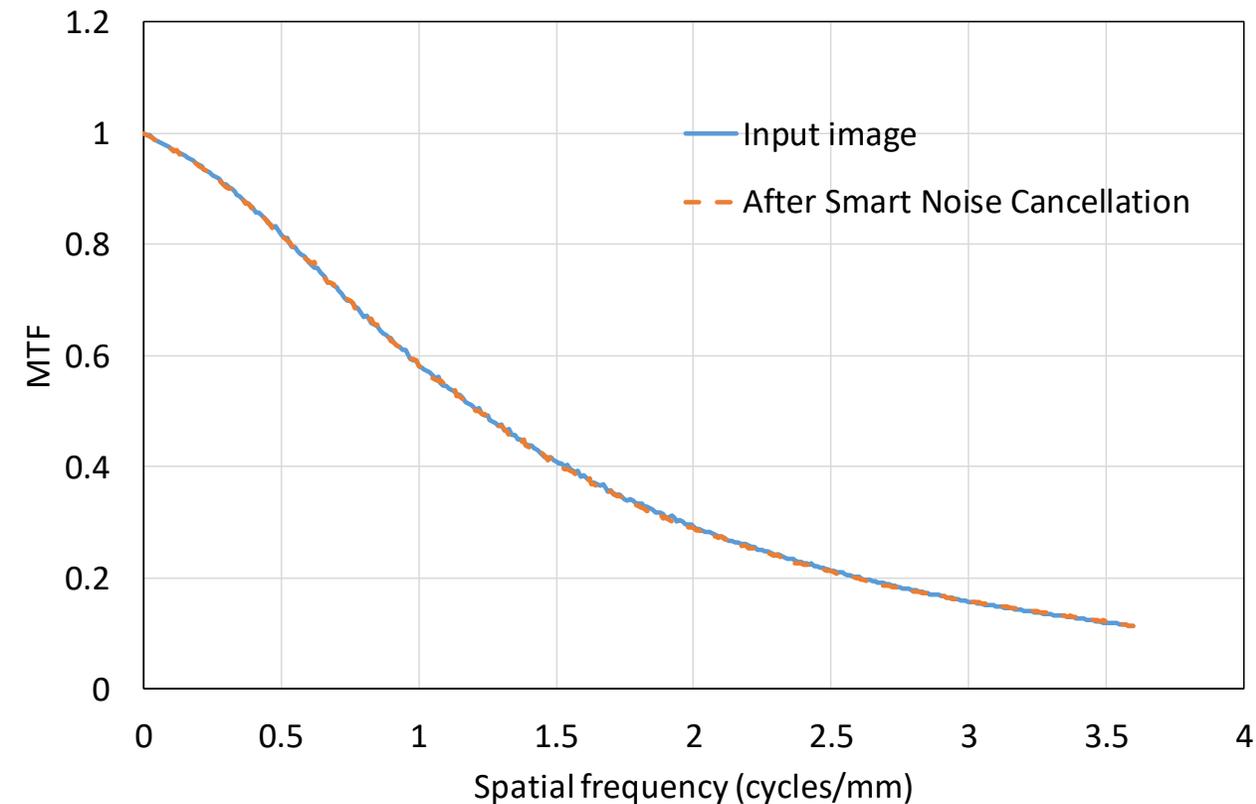
# Results – High Contrast Sharpness

- MTF was computed in linear exposure space before and after Smart Noise Cancellation
- RQA-5 beam
- There was no MTF loss after Smart Noise Cancellation



MTF phantom

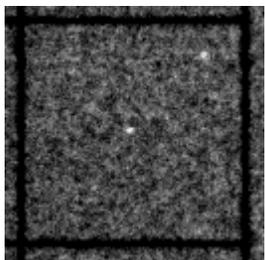
High-contrast sharpness is preserved with Smart Noise Cancellation



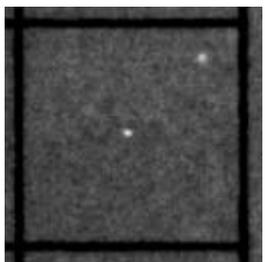
# Results – Contrast-Detail Analysis

- Contrast-detail curves and  $IQF_{inv}$  scores were obtained from the CDRAD Analyser 2.0 Software before and after Smart Noise Cancellation
- Quality score plotted as a function of air kerma at detector
- Improved detection after Smart Noise Cancellation, mainly for larger low-contrast features

## Scoring

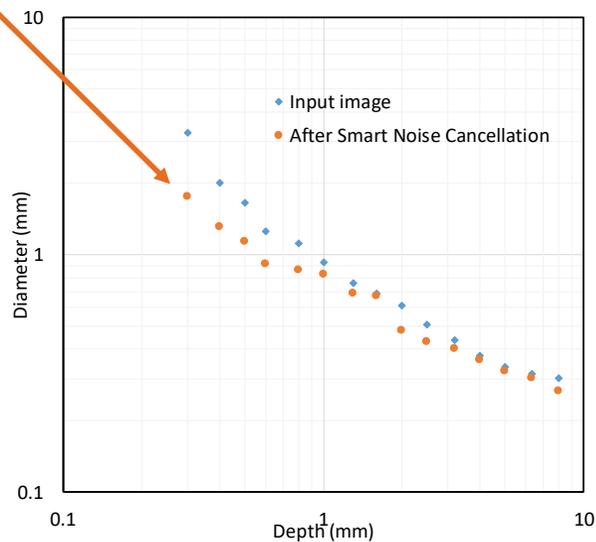


Input

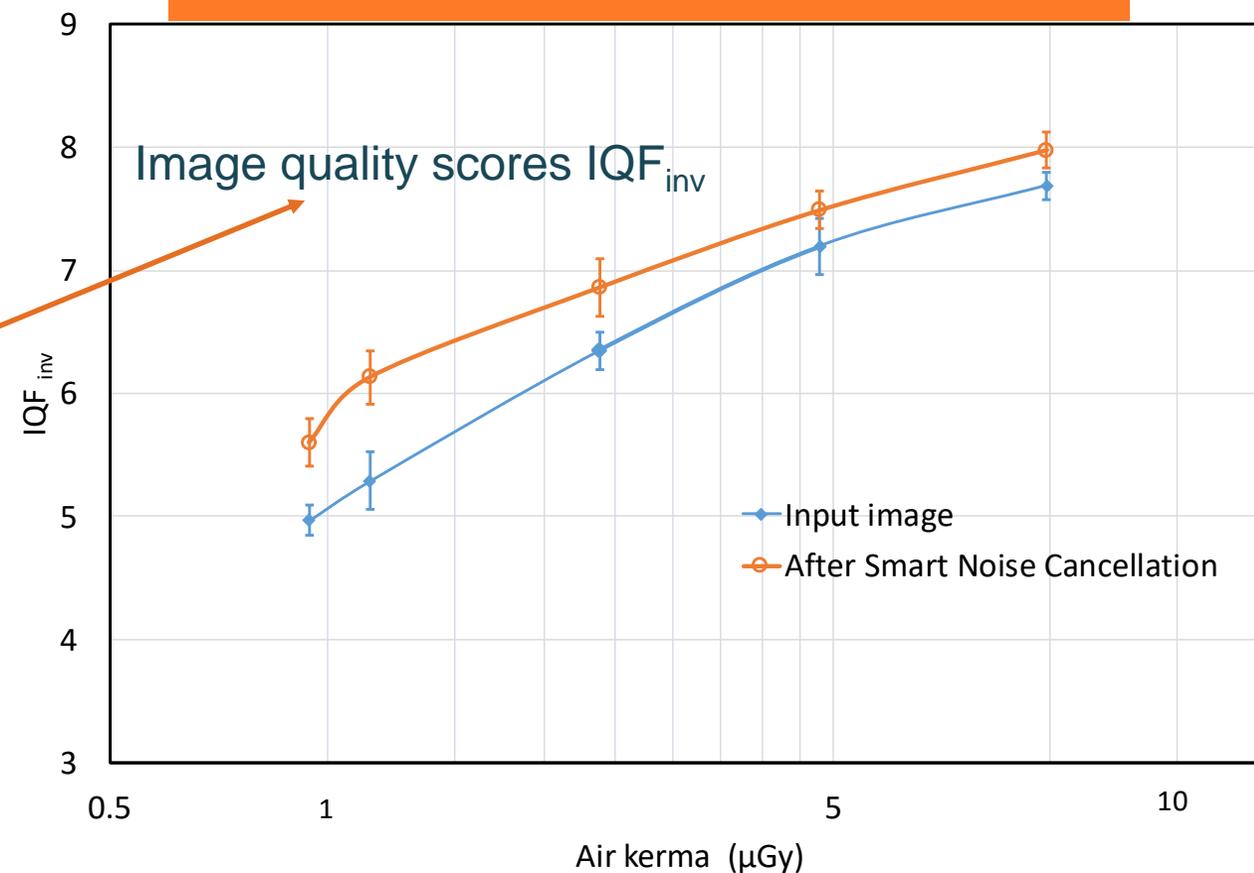


After Smart  
Noise  
Cancellation

## Contrast-Detail Curve



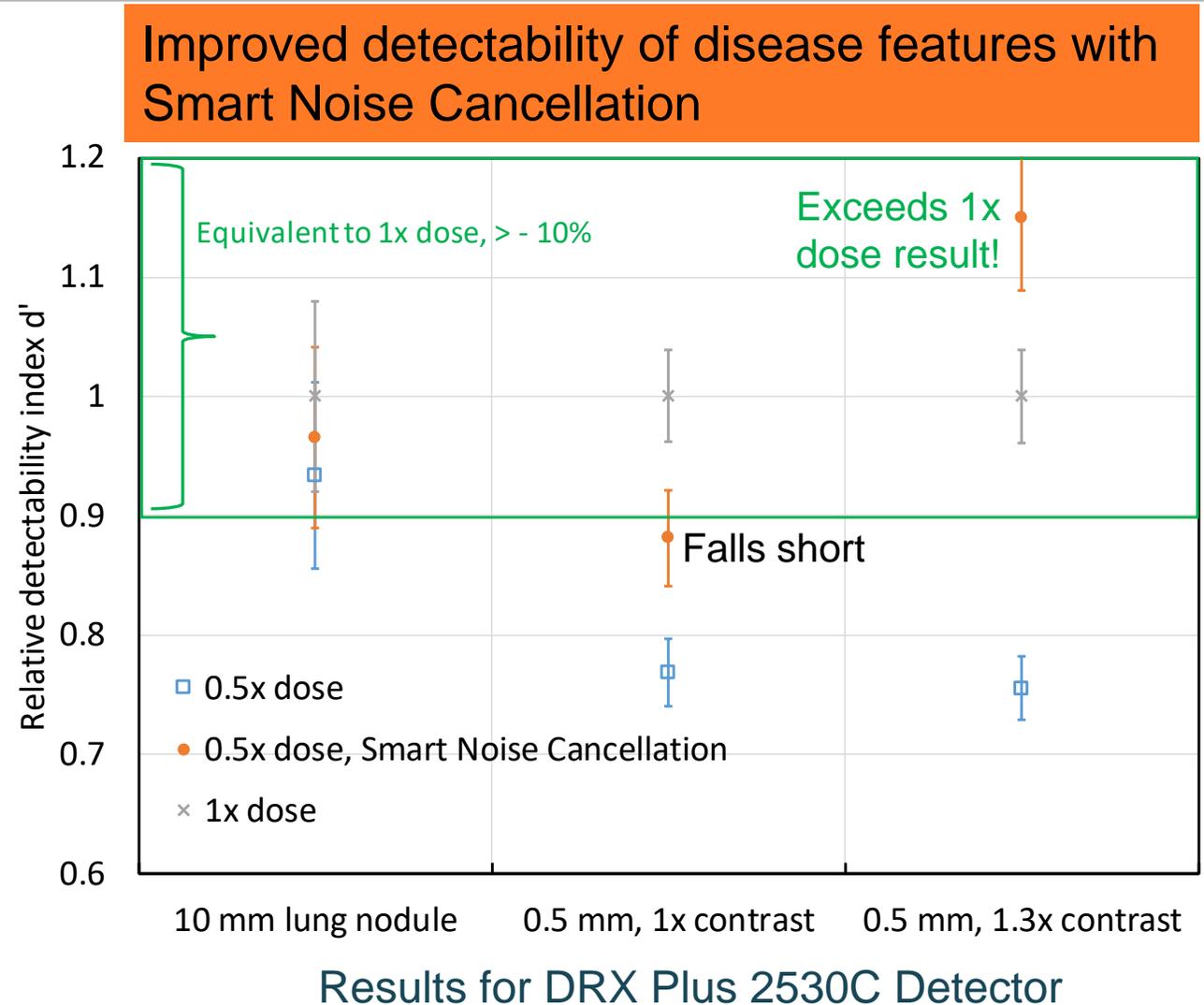
## Increased detection scores $IQF_{inv}$ with Smart Noise Cancellation



Carestream DRX Plus 3543C Detector, 70 kVp

# Results – Detectability of Disease Features, $d'$

- All data is normalized to the  $d'$  result for 1x dose, default image processing (gray symbol)
- A 10% loss in  $d'$  can be detected in larger reader study and is therefore significant
- The region between 0.9 and 1.2x in relative  $d'$  is marked by the green rectangle as at least equivalent to 1x dose
- Results support up to 2x dose reduction with Smart Noise Cancellation for larger features, e.g. 10 mm lung nodule, and the higher contrast small feature, see orange symbols relative to gray symbols.
- Smart Noise Cancellation is not able to recover disease features below threshold or increase visibility of features at threshold, see results for 1x contrast of the 0.5 mm feature



---

# IMAGE EXAMPLES

# Smart Noise Cancellation and Scatter Suppression

---

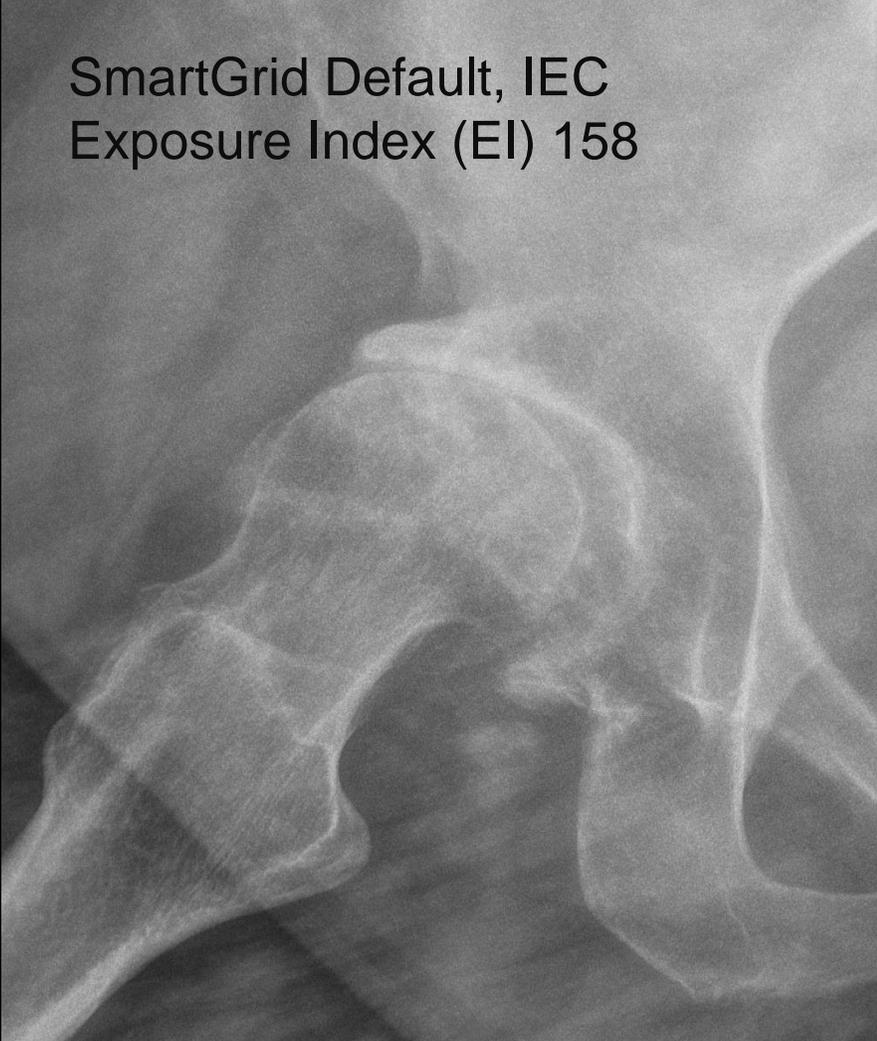
- Anti-scatter grids improve image quality by reducing the impact of scattered radiation
- Radiographs, however, are frequently acquired without grids due to challenges in grid alignment, x-ray cutoff, and workflow impact
- Software-based scatter suppression has been available in recent years\*
- While these solutions led to improvements in anatomy contrast, they also resulted in increased image noise
- The combination of scatter suppression software with Smart Noise Cancellation\*\* addresses the noise issue, leading to image quality equivalent to captures with grid, but at < 50% of the dose.
- Image examples show scatter suppression performance using three methods:
  - Physical grid (6:1 and 12:1 grid ratios)
  - SmartGrid (Carestream software-based scatter suppression)
  - SmartGrid+ (Smart Grid with Smart Noise Cancellation)

\* <https://www.carestream.com/blog/wp-content/uploads/2020/01/whitepaper-SmartGrid-Image-Quality-Impact.pdf>

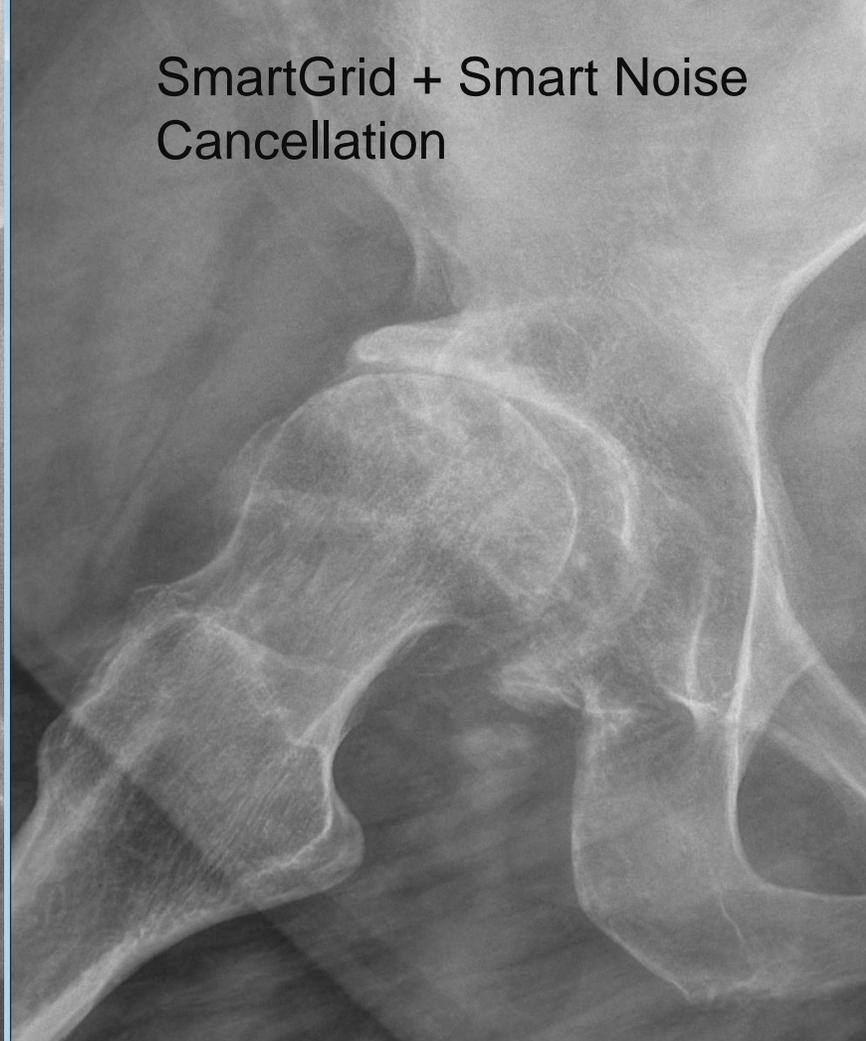
\*\* "Performance Comparison of Physical Anti-Scatter Grid and AI-Based Virtual Scatter Reduction Across Patient Size" - RSNA Featured Paper 20009415

# SmartGrid DRX Plus 3543C Clinical Case

SmartGrid Default, IEC  
Exposure Index (EI) 158



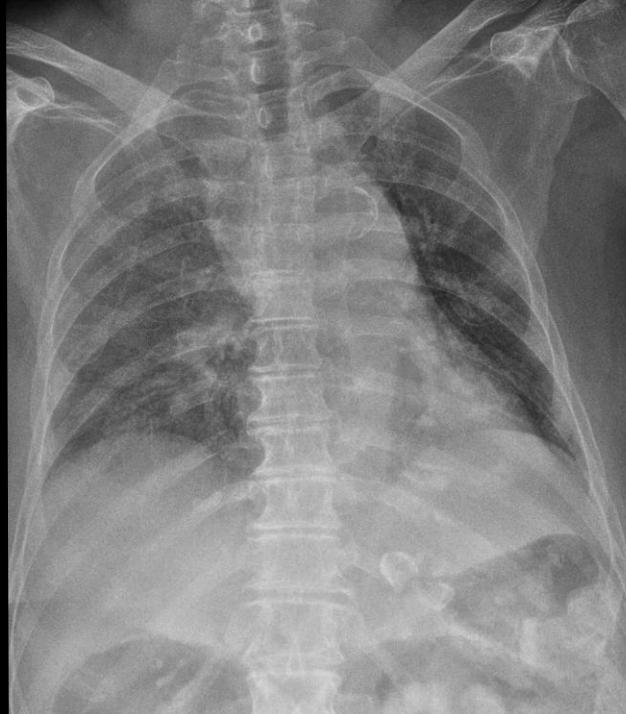
SmartGrid + Smart Noise  
Cancellation



Contrast enhancement  
and noise reduction



100 kVp, 0.5 mAs IEC EI 193.1  
Default



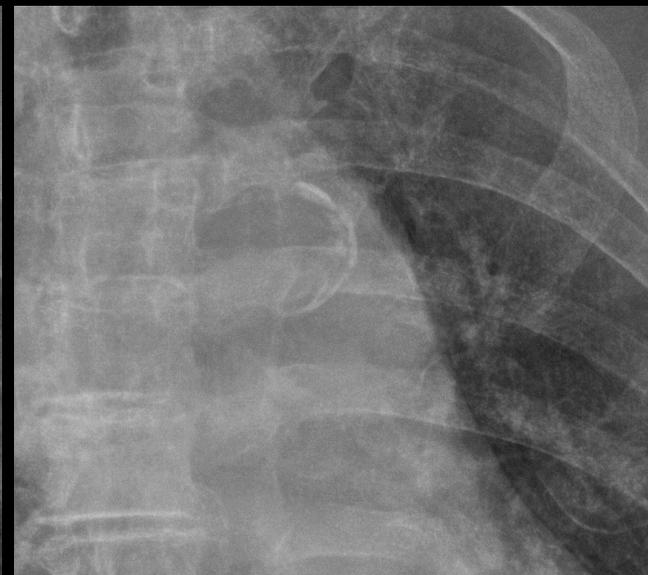
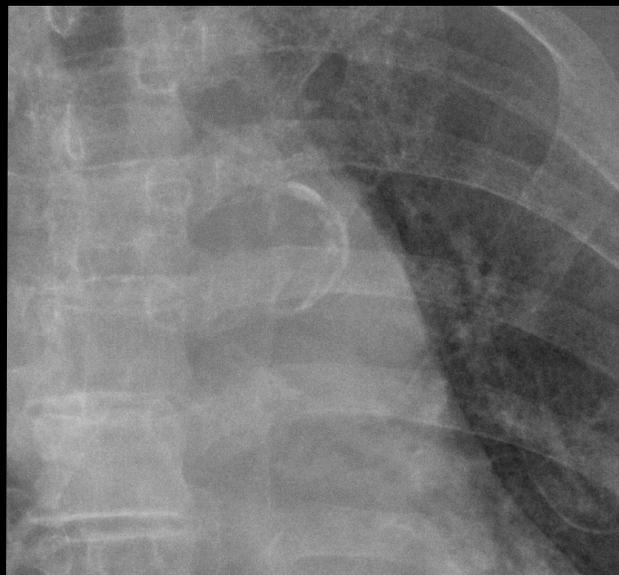
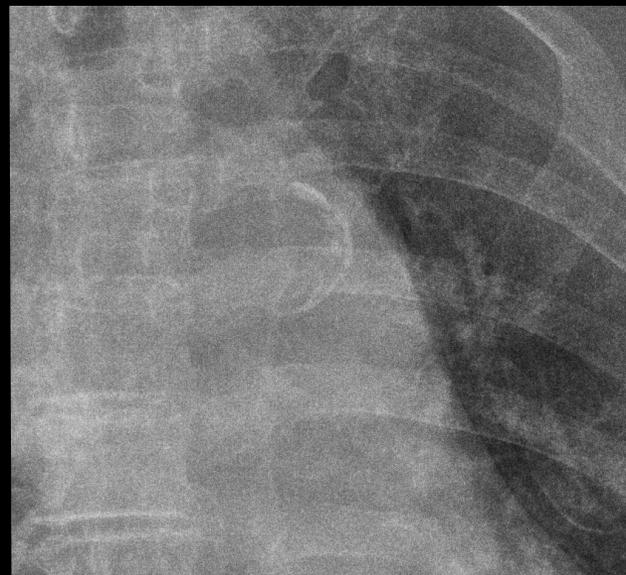
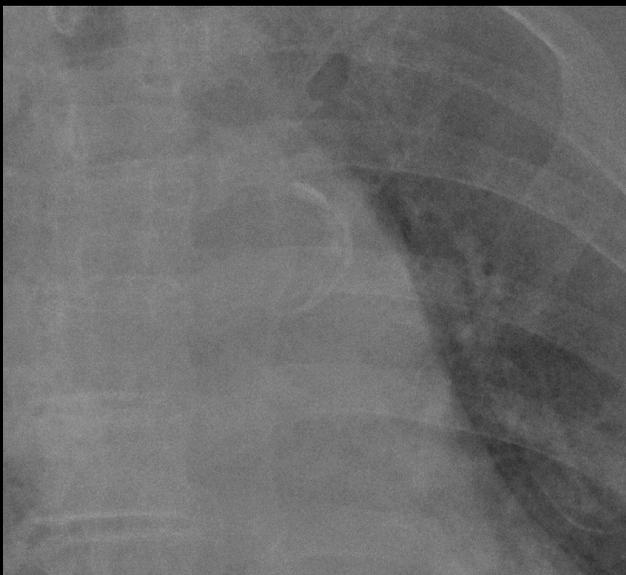
100 kVp, 0.5 mAs IEC EI 193.1  
SmartGrid



100 kVp, 1.2 mAs, 6:1 grid  
IEC EI 192.1 Default



100 kVp, 0.5 mAs, IEC EI 193.1  
SmartGrid + Smart Noise Cancellation



70 kVp 2 mAs, 40 In 6:1 grid



70 kVp 0.9 mAs, SmartGrid +  
Smart Noise Cancellation



70 kVp 0.9 mAs, SmartGrid



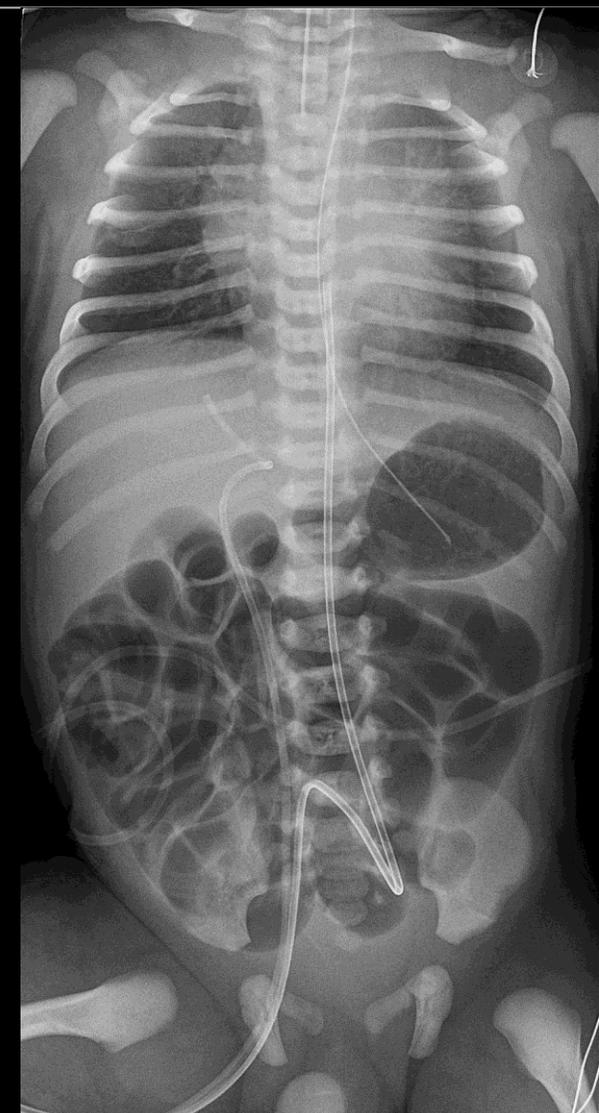
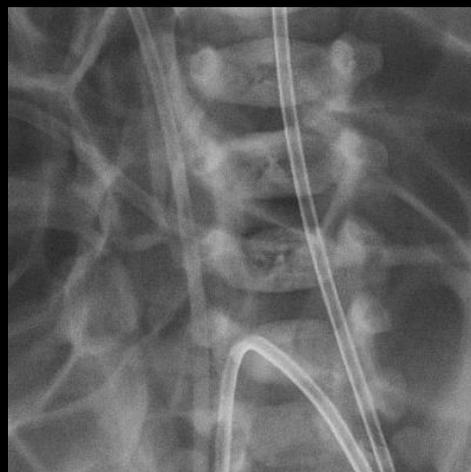
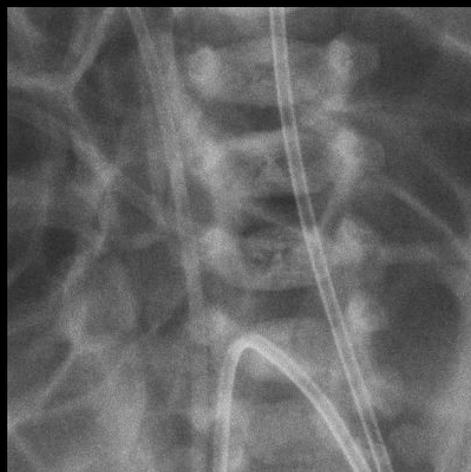
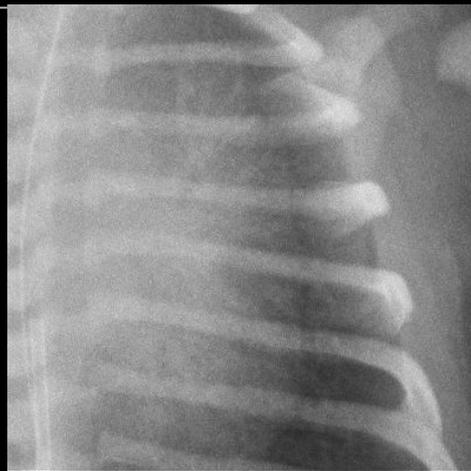
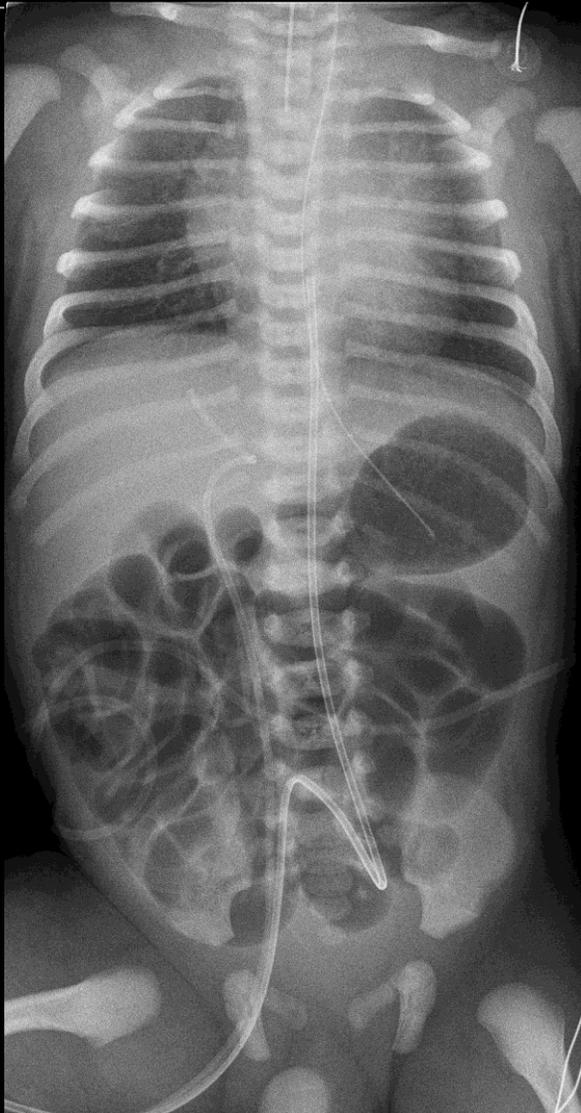
# Image Enhancement and Dose Reduction in Neonatal Imaging

---

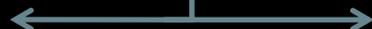
- Image enhancement and dose reduction are particularly important in the neonatal ICU
- The youngest, most vulnerable patients in terms of radiation, get imaged repeatedly to check for placement of tubes and lines and other changes
- The Carestream DRX Plus 2530C Detector was designed for this market with a smaller 98 micron pixel pitch and a cesium iodide scintillator, already providing excellent low dose performance and resolution
- The following slide shows how Smart Noise Cancellation can enhance these benefits even further; please note the low IEC EI of 80

# Smart Noise Cancellation, DRX Plus 2530C Detector

55 kVp 1 mAs IEC EI 80



Default

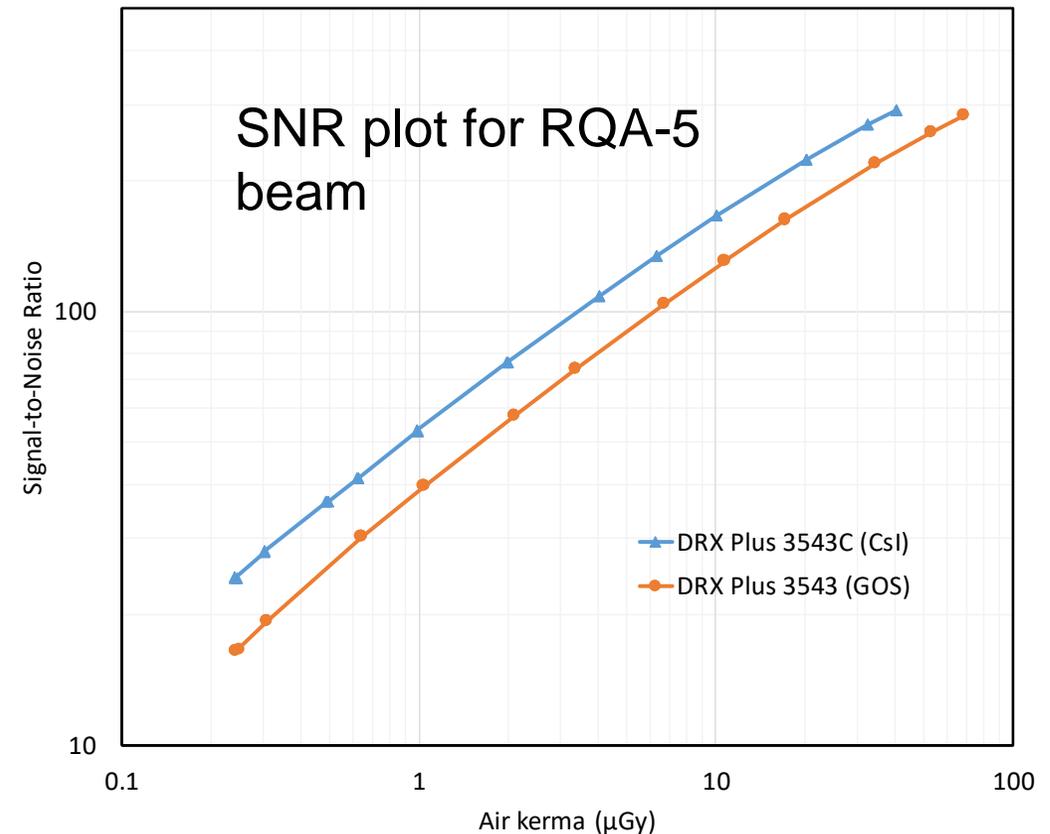


Smart Noise Cancellation

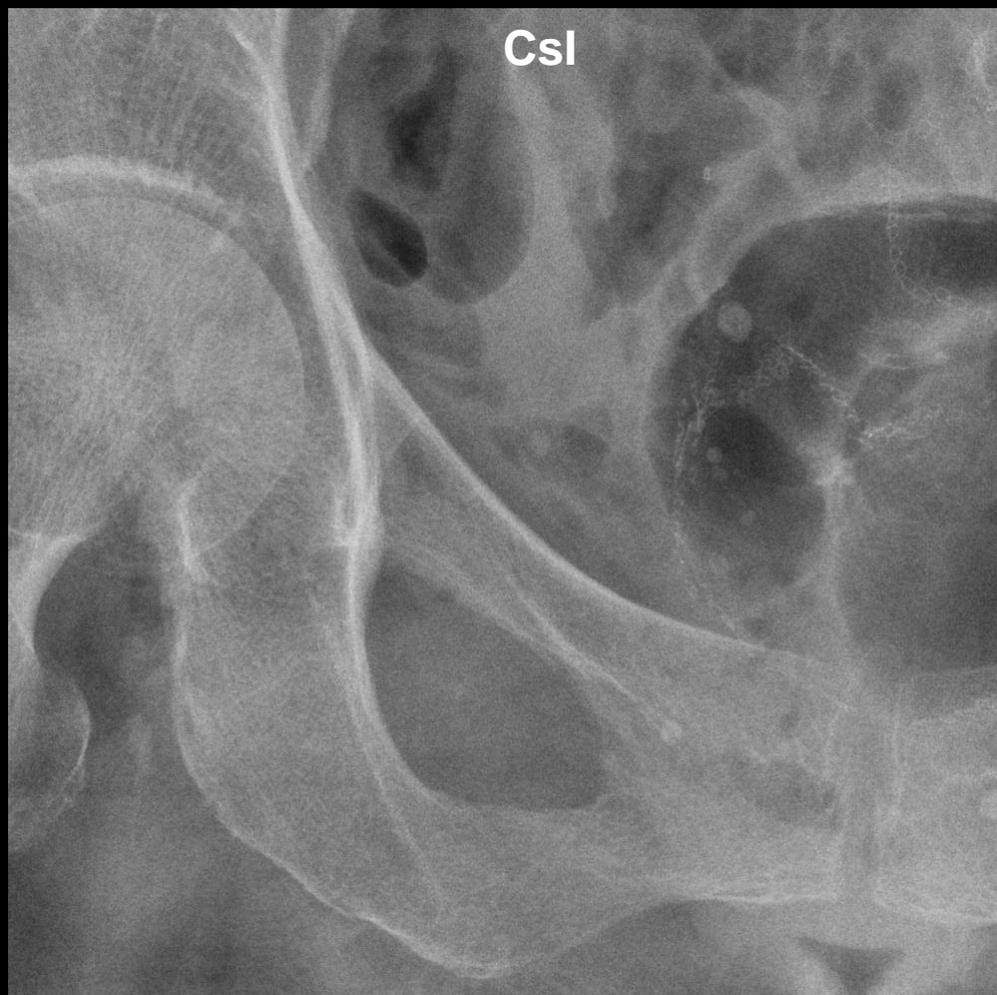
# Image Comparison of Scintillator Technology

- Carestream's detector portfolio has a choice of two scintillators
- Gadolinium oxysulfide (GOS) is a cost-effective offering with good image quality and reduced dose compared with computed radiography (CR)
- The cesium iodide (CsI) scintillator is a premium offering for the highest image quality and lowest dose
- Detectors with CsI have higher X-ray absorption and improved light management due to the columnar structure of the scintillator compared with GOS
- As a result, images on CsI have a higher signal-to-noise ratio (SNR) than images on GOS at the same input exposure (dose)

Eclipse with Smart Noise Cancellation on GOS detectors can produce equivalent image quality to Eclipse on CsI detectors at the same exposure



# CsI @ 500 speed $\neq$ GOS @ 500 speed

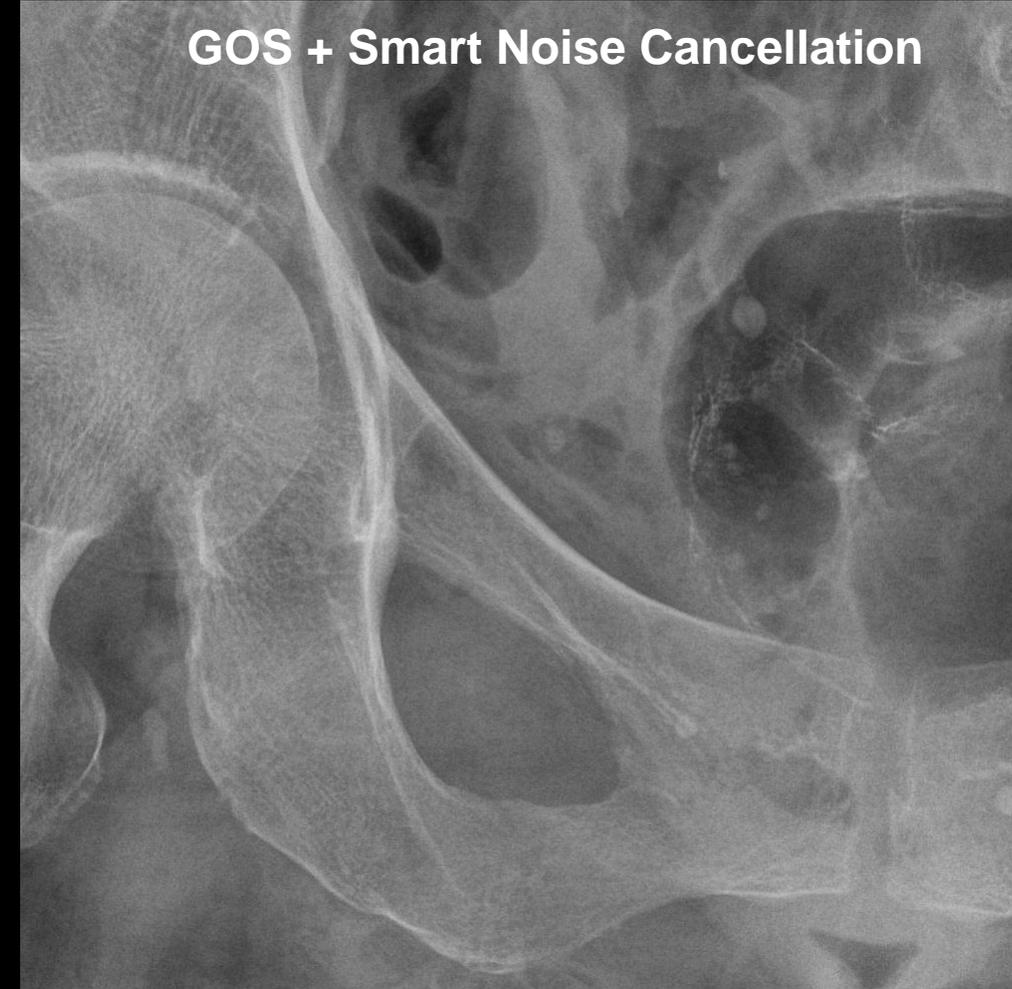
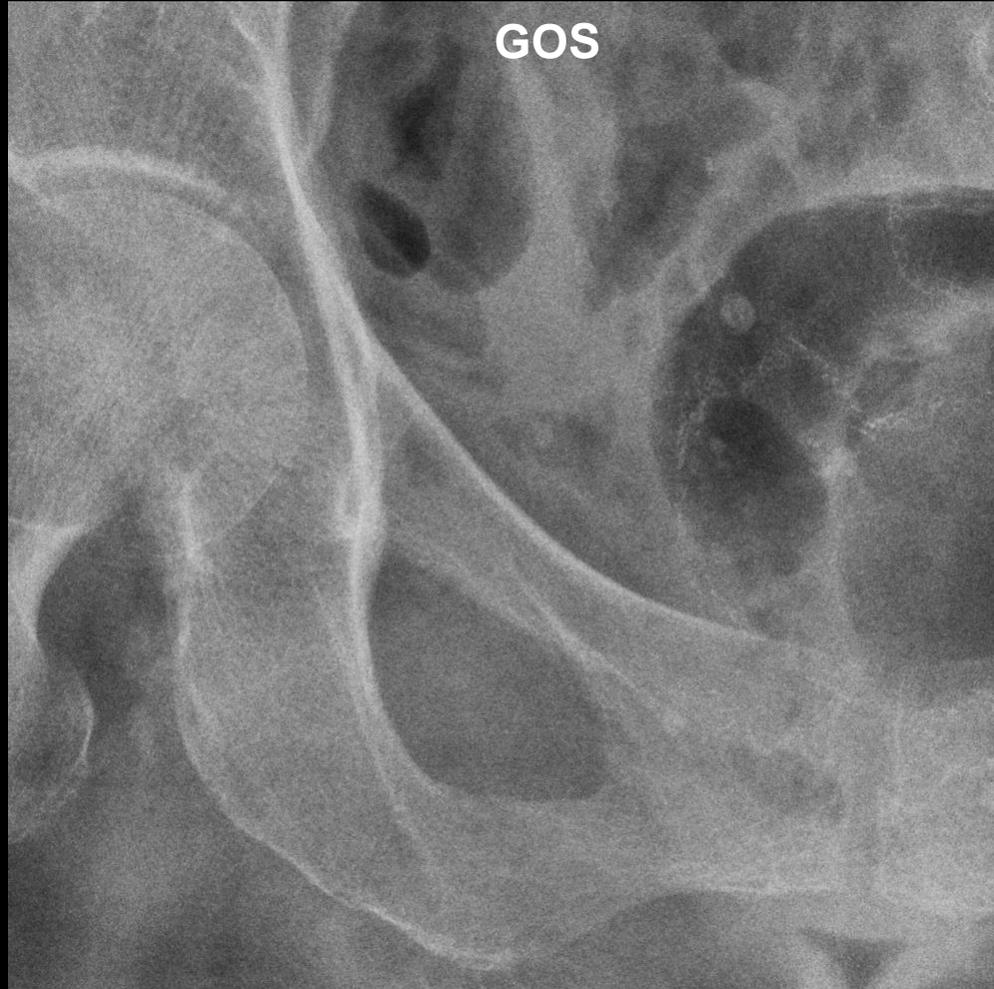


75 kVp 6.3 mAs, 40 In/cm 6:1 Grid, IEC EI 129



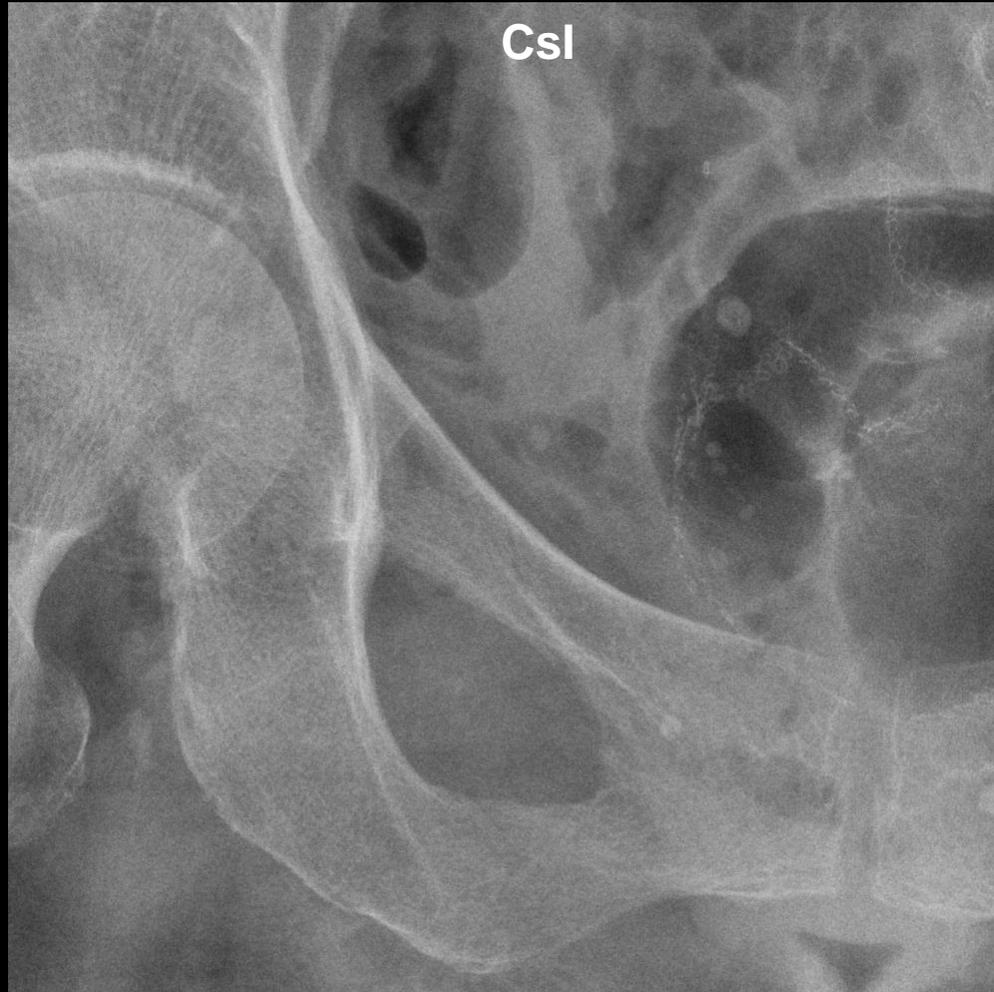
75 kVp 6.3 mAs, 40 In/cm 6:1 Grid, IEC EI 126

# GOS @ 500 speed – Smart Noise Cancellation Effect

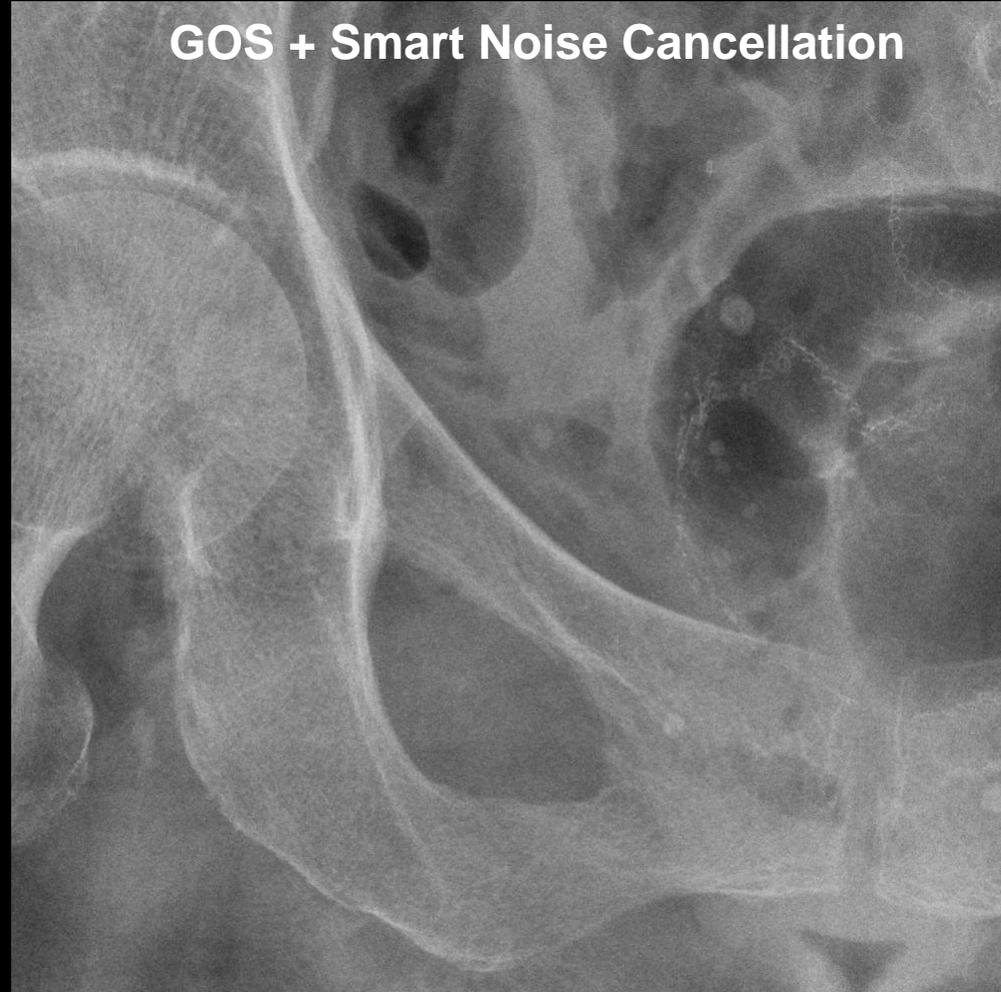


75 kVp 6.3 mAs, 40 In/cm 6:1 Grid, IEC EI 126

# CsI @ 500 speed = GOS @ 500 speed



75 kVp 6.3 mAs, 40 In/cm 6:1 Grid, IEC EI 129



75 kVp 6.3 mAs, 40 In/cm 6:1 Grid, IEC EI 126

# Carestream DRX-L Detector for Single Shot LLI



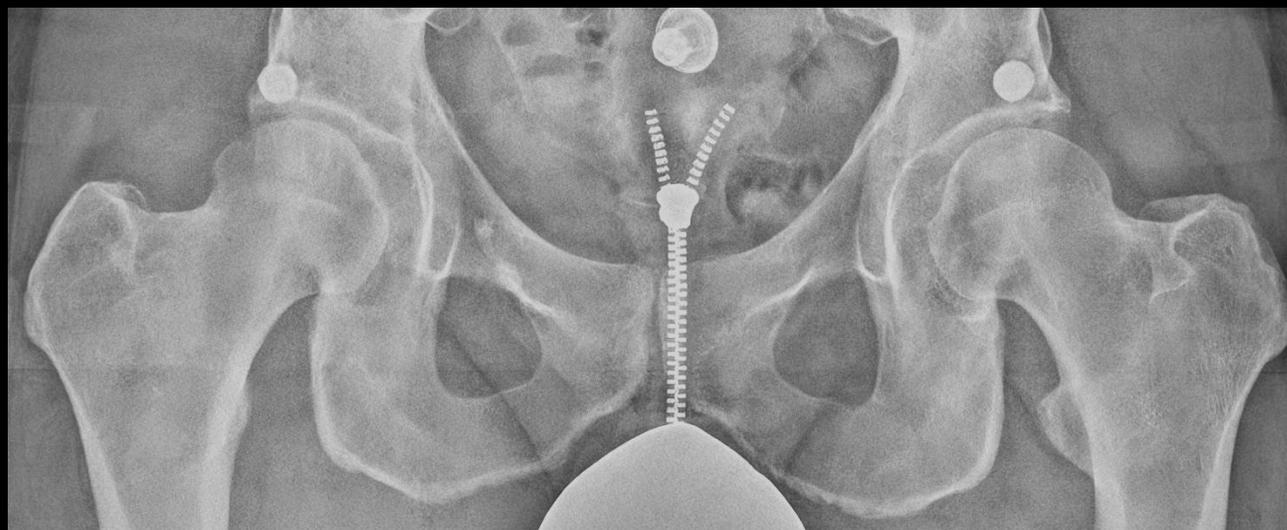
Eclipse, full image

Eclipse



Eclipse + Smart  
Noise Cancellation

This GOS based  
detector benefits from  
Smart Noise  
Cancellation for the  
lowest possible dose



# Summary and Conclusions

---

- The performance of a deep convolutional neural network in terms of noise reduction was characterized using anonymized clinical images, representative of general radiography and pediatrics, and a set of phantoms
- The network achieved:
  - 2 to 4x noise reduction in flat areas of the images, depending on exposure
  - Preservation of edge content and high contrast sharpness in the images
  - 10% to 20% improvement in contrast-detail scores on the CDRAD 2.0 phantom
  - Improvements in the detectability of disease features for a 10 mm lung nodule and a higher contrast 0.5 mm feature
- A comparison of the detectability index  $d'$  at 1x dose with Eclipse processing and at 50% dose with Smart Noise Cancellation and Eclipse suggests that up to 50% dose reduction can be achieved relative to the nominal setting (400 speed or 2.5  $\mu\text{Gy}$  for Csl detectors and 320 speed or 3.1  $\mu\text{Gy}$  for GOS detectors).
- Improvements in the image quality of clinical images with Smart Noise Cancellation and Eclipse image processing were demonstrated for:
  - A combination of Smart Grid scatter suppression software with Smart Noise Cancellation
  - Applications in the neonatal ICU
  - Detectors with GOS scintillator, which can achieve low noise positions traditionally only seen on detectors with Csl scintillator

**Carestream**